On the Z-Width Limitation due to the Vibration Modes of Haptic Interfaces

Jorge Juan Gil, Mildred J. Puerto, Iñaki Díaz and Emilio Sánchez

Abstract—This paper addresses the effect of internal vibration modes on the stability boundary for haptic rendering. A linear model that includes two vibration modes has been used to characterize one degree-of-freedom of the PHANToM 1.0 haptic interface, and predict the maximum achievable impedances for haptic rendering. The theoretical and experimental results show that the vibration modes of the mechanical interface significantly limit the Z-width of the haptic system.

Index Terms—Haptic systems, Stability, Vibration modes

I. INTRODUCTION

Haptic interfaces are becoming very popular as simulation tools in surgery [1], [2], industry [3], and education [4], among many other fields. Implementing a good haptic controller enables the user to obtain a proper tactile interaction with a virtual environment. However, a number of hardware and software limitations have yet to be solved to provide a high degree of realism.

Impedance-based haptic systems usually model a virtual body by means of a virtual spring. To simulate rigid contacts, the virtual stiffness $K$ is set as high as possible. Several studies [5], [6], [7] have found the dependence of passivity and stability limits on factors such as the sampling period, the viscous damping, and time delays. It has been proven that the addition of a virtual damper in parallel with the virtual spring allows the implementation of higher stiffness coefficients before leading to system instability [8], [9], [10], [11], [12]. This beneficial effect is also achieved by increasing the physical damping of the interface [13], [14], [15], [16].

In a haptic interaction with a virtual impedance that consists of a spring $K$ and damping $B$, the region containing the stable values of these parameters is called the Z-width of the haptic system [17]. The size and shape of this region can be used to compare the performance of different haptic devices. Therefore, a number of control strategies have been developed with the aim of increasing the Z-width of haptic systems, that is, the set of impedances that they can simulate [18], [19], [20], [21], [22]. The boundary of this stability region has been found experimentally in [12], [13]. Furthermore, it is interesting to note that some experimental studies [17], [18], [22] show that it is not possible to implement relatively high virtual damping coefficients. From a certain value of virtual damping $B$, the critical value of the virtual stiffness $K$ decreases drastically.

This paper shows that the vibration modes of the device are responsible for the limitation of the Z-width. The stable boundary is found by using a theoretical model of the system that includes the vibration modes. This study exhibits that the critical frequency of the system presents a discontinuity as the virtual damping increases, jumping to values above the resonance frequencies of the modes. Experiments that support the theoretical findings are also presented. To extend the validity of this analysis, several time delays have been introduced in both the theoretical models as in the experimental setup.

The well-known PHANToM Premium 1.0 haptic interface (Fig. 1) was used to analyze the influence of the vibration modes on the Z-width of the system. To compute the theoretical stability boundaries, a linear model for the mechanical interface—including the most significant vibration modes—is estimated in Section II. Next, the shapes of the theoretical stability regions are analyzed in Section III, while the experimental regions are shown in Section IV. Finally, some conclusions and future work are reported in the last section.

II. DEVICE MODEL IDENTIFICATION

This section proposes a linear model for the mechanical interface including its most significant vibration modes. The study is limited to the first degree-of-freedom of the PHANToM ($\phi$-axis in Fig. 1). Only the motor that acts on
Locking bolts

Fig. 2. Four locking bolts are placed on both sides of the non-active motors of the PHANToM to avoid undesired reconfigurations of the device during the experiments.

![Bode Plot](image)

Fig. 3. Experimental (blue line) and theoretical (black line) Bode diagrams for the PHANToM.

this axis is active. To avoid undesired reconfigurations of the rest of the device, the other motors are mechanically locked (Fig. 2). Moreover, the stylus of the PHANToM has been removed to avoid the influence of mobile parts on the device.

The transfer function that characterizes the interface was estimated from the frequency response of the device to a white noise input signal [23]. This type of actuation allows the excitation of a wide range of frequencies and the identification of the first vibration modes of the system.

The white noise signal was generated by a Simulink® block and commanded to the active motor by a dSPACE DS1104 board running at 1 kHz. This board also read the encoder information. The white noise signal successfully excited the system from 0.7 Hz up to 300 Hz over thirty seconds. The lower frequency was set near the limit imposed by the length of the window used in the data analysis (4096 sampling points that allow a smooth frequency response), while the upper limit was set below the Nyquist frequency and the bandwidth of the actuators.

Fig. 3 shows the frequency response of the PHANToM to the white noise signal. Several vibration modes (at least four) arise below 300 Hz. To manage a relatively simple model, only the first two vibration modes were modeled. The first one (at approximately 80 Hz) is a structural mode of the mechanism, while the second one (close to 200 Hz) is due to the transmission cable. The suggested transfer function for the interface is

$$G(s) = \frac{1}{ms^2 + bs + c}$$

where $m$ is the inertia of the rotor, $b$ is the damping, and $c$ is the elastic constant.

The system model proposed in the previous section was used to obtain the theoretical stability boundaries of the haptic interaction. A block diagram of the haptic device colliding with a virtual wall is shown in Fig. 5.

Transfer function $G(s)$ is the theoretical model for the device with two vibration modes (1). To be consistent with

![Mechanical Model](image)

Fig. 4. Mechanical model for the device with two vibration modes.

From this, ten parameters are necessary to model the interface with two vibration modes. Following an approach similar to the one presented in [23], these parameters could be related to the ten parameters depicted in Fig. 4 for a physical interpretation. Using that nomenclature, it is possible to see that $m_1$ exactly corresponds to the inertia of the rotor, which is the place where motor’s force $F$ actuates and where the encoder measures the device’s position $X$. Coefficients $k_{11}$ and $b_{12}$ model the transmission cable, and $k_{23}$ and $b_{23}$ model a structural mode of the mechanism. However, the ten parameters presented in (1) are more convenient for the identification process.

Parameters of $G(s)$ can be fit manually or by using least-square iterative methods to match the experimental data. Table I reports the obtained parameters, and Fig. 3 depicts the discrete-time Bode diagram for $G(s)$ together with the experimental response. Although only two vibration modes have been modeled, it is clear that the theoretical transfer function properly models the dynamics of the device.

### III. Theoretical Stability Boundaries

The system model proposed in the previous section was used to obtain the theoretical stability boundaries of the haptic interaction. A block diagram of the haptic device colliding with a virtual wall is shown in Fig. 5.

Transfer function $G(s)$ is the theoretical model for the device with two vibration modes (1). To be consistent with
the acquisition rate of the control board, the sampling period $T$ was set to 1 ms. The impedance of the virtual contact consisted of a virtual stiffness $K$ and a virtual damping $B$. Before the zero-order holder $H(s)$, a discrete time delay $z^{-d}$ was included to obtain several stability regions with the same device, as it was performed in [24]. Furthermore, the presence of time delay makes the model more complete, since actual haptic systems always suffer from a certain inherent delay due to computation or amplification processes.

The characteristic equation of the system is

$$1 + z^{-d} \left( K + B \frac{1-z^{-1}}{T} \right) Z[H(s)G(s)] = 0,$$

where $Z[\cdot]$ is the $Z$-transform of the transfer function within brackets. The critical stiffness $K_{CR}$—as a function of the virtual damping and the time delay—can be found by calculating

$$K_{CR} = \text{Gm}\{ \frac{Z[H(s)G(s)]}{z^d + B \frac{1-z^{-1}}{T} Z[H(s)G(s)]} \},$$

where $\text{Gm}\{\cdot\}$ is the gain margin of the transfer function.

Stability regions can be found for different time delay conditions by computing (4) over a range of virtual damping values. The results for three different time delays ($t_d = 2$, 4 and 8 ms) are shown in Fig. 6. As an example, the Matlab® code to obtain the stability boundary of the PHANToM for a delay of 2 ms is reported in Appendix I.

Notice in Fig. 6 that two different parts can be clearly distinguished for each delay. For small values of virtual damping (part I), the critical stiffness increases with $B$ up to a maximum value $K_{CR}^{\text{max}}$ for $B_i$. However, for virtual damping coefficients higher than $B_i$ (part II), the critical stiffness decreases with $B$. Therefore, the well-known assertion that the virtual damping positively contributes to the stability of the system [8], [10] is true, but limited to a specific range of values.

The critical frequencies of the system for each delay are also reported at the bottom of Fig. 6. The abrupt truncation of the stability region after transition point $B_i$ (part II) occurs when the critical oscillation frequencies jump to higher values. The critical frequency (called “ultimate frequency” from here on) corresponds to the phase crossover frequency of the Bode diagram of transfer function within brackets in (4), which varies with the virtual damping and time delay.

It is interesting to note that the stability region does not always decrease with the delay in the loop. In theory, as stated in [12], the stability region becomes smaller if the time delay increases. However, the stability region with a
time delay of 4 ms is larger than the stability region with 2 ms (Fig. 6 top). This unexpected result will be corroborated experimentally in Section IV. The explanation of this behavior cannot be, among others, neither the saturation of the actuator nor the sensor quantization, because the theoretical linear model does not include those limitations. Although the actual reason is not investigated in this study, it seems to be related with the fact that the transition point \( B_t \) sometimes reaches a frequency level above the first vibration mode (with time delays of 2 and 8 ms), and other times above the second vibration mode (time delay of 4 ms).

Related work [17], [18], [22] has previously found experimentally that for large values of virtual damping, the critical stiffness of the system decays abruptly. The haptic model proposed in this paper has included two vibration modes in order to find the theoretical explanation for this phenomenon and depict the stable region much more accurately. Fig. 7 shows the stability regions obtained using the theoretical model with and without vibration modes. In both cases, the delay was set to 2 ms. The vibration modes of the interface impose an important restriction in the \( Z \)-width of the PHANToM. Notice that the influence of the vibration modes also affected part I of the boundary: in this case, the critical stiffness was higher when the vibration modes were included.

### IV. Experimental Stability Boundary

The critical values for the virtual stiffness of the PHANToM were experimentally obtained to validate the theoretical boundaries shown in the previous section. The critical limits were found by using the relay method [10], [25], [26]. This method consists of a relay feedback—an on-off controller—that makes the system oscillate around a reference position.

In steady state, the relay force is a square wave, the output position is similar to a sinusoid wave, and they have opposite phases (Fig. 8). It can be demonstrated [25] that the ultimate frequency \( \omega_{CR} \) is the oscillation frequency of both signals, and the critical gain is the quotient of the amplitudes of the first harmonic of the square wave and the output position. The oscillation frequency is found by determining the maximum peak of the average power spectral density of both signals in steady state. The gain margin is obtained by evaluating the empirical transfer function (\texttt{fitestimate} Matlab function using input-output signals) at the oscillation frequency.

The testbed description and kinematic configuration are the same as in Section II. The reference for the relay force transition was placed approximately at the middle of the available workspace. Input force was applied to the active motor, and the position of the device was measured. In each relay experiment, all signals were measured for more than
15 seconds (in steady state).

To obtain the critical values for different damping coefficients and delays, the relay force was not directly commanded to the device. The viscous force due to the virtual damping was added to the relay force, and then both of them were delayed (Fig. 9 bottom). This way, the relay method obtained the critical gain (4).

As in previous section, time delay was artificially set to 2, 4 and 8 ms. Without any delay in the loop, it is not possible to obtain the complete stability region experimentally because the actuator becomes saturated. Table II and Fig. 10 present the oscillation frequencies and gain margins of the 26 experiments performed. Fig. 10 shows that the theoretical results depicted in Fig. 6 fit quite well with the experimental data. This data allows the two parts of the stability region to be identified and shows the truncation of the boundary at a certain damping value.

V. CONCLUSIONS AND FUTURE WORK

This paper presents the basis for a better understanding of the influence of the vibration modes on the Z-width of a haptic system, that is, the set of stable parameters that can be simulated—usually a \((K, B)\) pair. The theoretical and experimental results confirm that the vibration modes of the mechanical interface drastically decrease the Z-width of the system, and impose an upper limit on the virtual damping coefficient \(B\) that can be implemented.

The existence of this limit was already known experimentally in the field of haptics. Several authors [17], [18], [22] had found the stability regions of different haptic devices, showing the abrupt truncation of the Z-width of the system at a certain damping point. However, none of them could predict the shape of the boundary a priori. Although this paper does not provide a theoretical expression for the maximum achievable damping coefficient \(B\), it has demonstrated the possibility of numerically determining the stability boundaries for one degree-of-freedom of the PHANToM 1.0 haptic interface. To obtain this result, a linear transfer function with two vibration modes was identified.

Future work will more deeply investigate the effect of time delays in the Z-width limitation due to vibration modes, and more specifically why the system changes its ultimate vibration frequency with delays will be analyzed. The theoretical analysis and results will also be extended to other devices and kinematic configurations.

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<th>(K_{CR}) (Nm/rad)</th>
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Fig. 10. Critical stiffness (top) and ultimate frequencies (bottom) as a function of the virtual damping for different time delays.
APPENDIX I

Matlab® code used to depict the stability region (Fig. 6) of the PHANToM with 2 ms of delay:

```matlab
G0=tf(856,[1 5 0]);
G1=tf(2296*[1 80 174400],1744+[1 83 229600]);
G2=tf(13440*[1 90 298800],2988+[1 352 1344000]);
G=G0*G1*G2;
T=0.001;
z=tf([1 0],1,T);
Gz=z*cd2d(G,T);
vector=0:0.001:0.099;
K2ms=vector*0;
W2ms=vector*0;
n=0;
for B=vector,
    n=n+1;
    [Q,F,WQ,WF]=margin(T/(((T*z*z)/Gz)+B*(z-1)/z));
    K2ms(n)=Q;
    W2ms(n)=WQ/(2*pi);
end;
B=vector;
plot(B,K2ms);
figure;
plot(B,W2ms);
```

REFERENCES


